

Biomedical Image Processing Technique Using N Cut Theorem

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Abstract

Computerized or automatic detection of tumors in medical images is inspired by inescapably of high accuracy when it is dealing with human life. This sickness has been the focal point of consideration of thousands of analysts for a long time, all throughout the planet. Specialists have joined their information and endeavours from numerous spaces going from clinical to numerical sciences, to all the more likely comprehend the infection also, to discover more viable medicines. The computer abetment is very important in medical institution because it could ameliorate the result of different types of disease recognition and the result of negative cases should be very low. MRI is often used for the distinguishing proof of different inconsistencies in delicate tissues, for instance, the Spine, injuries, and tumors. So, the processing of Magnetic Resonance Imaging (MRI) is one of the techniques to detect tumor accurately. In image processing 3D image generation process simulated. The key objective of this paper is to detect and extract spine tumor from the patient MRI scanned images of the spine. In this cycle the progression incorporates are pre handling, figuring space of cross segment, recognizing limit of cross segment, detecting tumor affected area and calculation of the tumor area. This whole application process is developed using Matrix Laboratory (MATLAB).

Keywords

Spine Tumor, MRI, Binary Image, Gray Scale Image, MATLAB

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1. Introduction

Spinal tumor, it is defined as an abnormal growth of cell in the tissue within or surrounding the spinal cord and spinal column. There are two types of tumor such as: [1]

1. Benign (non-cancerous) tumor
2. Malignant (cancerous) tumor.

The Malignant tumor is divided into two parts:

1. Primary tumor
2. Secondary tumor.

In primary tumor, it originates in spine or spinal cord and the result of Metastatic or Secondary tumor from cancer extending from another side of the spine. The beginning of life threatening cancer tumors from a single cell that has embraced a chromosomal or hereditary change which influenced its protein adjust and expanding its capacity for mitotic division or diminishing the concealment instrument for cell division [2]. As dangerous cell misfortunes its typical capacity it begins it abnormal division much faster than surrounding normal tissue. The results of small mass of malignant cell is that single dividing cell and begins to seize adjacent normal tissue intimidate the damaged organ [3].

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To detect tumor multiple process is followed including MRI scan. Magnetic Resonance Imaging (MRI) scan is a technique to construct high quality of images of human body structure which is similar to the X-ray. But when we use MRI scan in spine then it dispense high information of spine which helps to detect and biomedical researching. The scanned values of MRI are splendid by its automated and more accurate classification [4]. MRI is primarily used to examine the internal organs for abnormalities such as tumor and chemical imbalances. MRI scanner is a large doughnut-shaped magnet. Patients are placed in a magnetic field. Amid the examination radio waves control the attractive position of particles of the body [13]. It is picked up by a powerful antenna and sent to the computer. After millions of calculation computer detect the RF signal and reconstruct the image. This image converted into 3-D (three-dimensional) image of the scanned area. This helps to identify the problems of the spine [5-8].

In this paper a fully automated method is proposed to detect spine tumor where MR picture examined as an input. Then, at that point it will be taken care of utilizing picture handling device of MATLAB. It is automatically detected any type of tumor which is available in human body then the percentage of tumor affected area will be calculated. If there is no tumor available then the users tell that “there is no tumor”.



Figure 1. Spine tumor.

2. Methodology

There are three stages in this algorithm, first step is pre-processing of given MRI image second step is morphological operation perform third step is showing the performing parameter and final step is calculating the tumor affected area. The steps of algorithms are [9-12]:

1. Load the image and resize it.
2. Region of interest (ROI) detection.

3. Segmentation of the image into four clusters.
4. Sort the clusters in descending order according to their means.
5. Update the cluster masks by the detected ROI in step 2
6. Spinal cord mask detection by f_1 , f_2 , f_3 and f_4 fitness functions
7. Tumor mask detection using the updated cluster mask no. 1 and the
8. Calculating the area of tumor.

a) Load the image and resize it:

To peruse a picture for preparing we have utilized the 'imread' order. The model peruses one of the example pictures 't.bmp' and stores it in an exhibit named I.

```
I = imread('t.bmp');
```

The record (sample image) isn't the current coordinator so we need to count the full way with document name. The content string '.bmp' counts the arrangement of the record by its standard document expansion. For instance, we can determine '.gif' for Graphics Interchange Format documents. To see a rundown of upheld designs, with their document expansions, the 'informat' capacity can be utilized. In the event that 'imread' can't discover a document named 'filename', it searches for a record named 'filename.fmt'.

```
imshow(I)
```

imshow(I) displays the grayscale image figure 1. Where imshow enhances figure, tomahawks, and picture object properties for showing the picture and stored image in the graphics file specified by filename. title(txt) adds the specified title to the axes or chart returned by the gca command. Reissuing the title command causes the new title to replace the old title.

```
I=imresize(I,[256 256])
```

B = imresize (A, [numrows numcols]) returns picture B that has the quantity of lines and sections determined by the two-component vector [numrows numcols].

```
I=im2double(rgb2gray(I))
```

I2 = im2double(I) converts the intensity image I to double precision and rescaling the data if necessary.

```
J = rgb2gray (I);
```

'rgb2gray' order changes over real nature picture to grayscale force picture. 'rgb' signifies Red, Green and Blue. The splendor level of rgb parts addressed decimal number from 0 to 255 or parallel 00000000 to 11111111. In Grayscale picture dark tone is addressed by R = G = B = 0 or R = G = B = 00000000 and white tone is addressed by R = G = B = 255

or R = G = B = 11111111. This imaging technique is called 8-bit grayscale.

`[h,w]=size(I)`

`[h,w]=size(I)` returns the lengths of the queried dimensions of I separately.

b) Region of Interest (ROI) detection:

`edge_mask=edge(I)`

`BW = edge(I)` returns a binary image BW containing 1s where the function finds edges in the input image I and 0s elsewhere. By default, edge uses the Sobel edge detection method.

`x=regionprops(edge_mask,'Solidity','Area','Image','BoundingBox','ConvexArea','Extent')`

`stats = regionprops (BW, properties)` returns measurements for the set of properties specified by properties for each 8-connected component (object) in the binary image, BW stats is struct array containing a struct for each object in the image.

`th2=ceil(mean(barea.*[1-bsol]))`

`Y = ceil(X)` rounds each element of X to the nearest integer greater than or equal to that element.

`se = strel('disk',th2)`

A strel object addresses a level morphological organizing component and it is a fundamental piece of morphological widening and disintegration tasks. A level organizing component is a twofold esteemed area, where the True pixels are remembered for the morphological calculation either 2-D or multidimensional and the bogus pixels are not. The middle pixel of the organizing component, called the beginning, which is distinguish the pixel in the picture being prepared. `SE = strel('disk',r,n)` makes a circle formed organizing component, where r indicates the span and n determines the quantity of line organizing components used to estimated the plate 63 shape. Morphological tasks utilizing circle approximations run a lot quicker when the organizing component utilizes approximations.

`closeBW = imclose(edge_mask,se)`

`J = imclose(I,SE)` performs morphological shutting on the grayscale or parallel picture I, returning the shut picture, J. SE is a solitary organizing component object returned by the strel or offsetstrel capacities. The morphological close activity is a widening followed by disintegration, utilizing the equivalent organizing component for the two tasks.

`temp=zeros(h,w)`

`X = zeros(sz1,...,szN)` returns a sz1-by-...- by-szN exhibit of zeros where sz1,...,szN demonstrate the size of each measurement.

c) Segmentation of the image into four clusters:

`I_re=reshape(I,[h*w 1])`

`B = reshape(A,sz)` reshapes A using the size vector, sz, to define size(B)

`labels_re=medfilt2(labels_re,[3 3])`

`J = medfilt2(I,[m n])` performs middle sifting and each yield pixel contains the middle worth in the m-by-n neighborhood around the comparing pixel in the information picture.

`labels_gray=rgb2gray(label2rgb(labels_re))`

`RGB = label2rgb(L)` changes over a mark grid, L, for example, those returned by labelmatrix, bwlabel, bwlabeln, or watershed, into a RGB shading picture to imagine the named locales. The label2rgb work decides the shading to dole out to each protest dependent on the quantity of items in the mark grid. The label2rgb work picks tones from the whole scope of the shading map.

d) Sort the clusters in descending order according to their means:

`cluster_stat(idx,:)= [idx mean(temp) var(temp) max(temp) min(temp) numel(temp)]`

Average or mean value of array.

`[~,idx]=sort(cluster_stat(:,2),'descend')`

This command Sorts array elements. `B = sort(A,dim)` returns the sorted elements of A along dimension dim.

`title(['Mask for sorted cluster no. ', num2str(idx)])`

`s = num2str(A)` command converts a numeric array into a character array which represents the numbers.

e) Update the cluster masks by the detected ROI in step 2:

`updated_mask=zeros(h,w,no_cluster)`

`temp=zeros(h,w)`

`X = zeros(1,3,'uint32')`

`X = 1*3 uint32 line vector`

`0 0 0`

`temp(labels_re==cluster_stat_sorted(idx,1) & closeBW==1)=1`

This command Perform a morphological close operation on the image.

`subplot(1,no_cluster,idx)`

`imshow(temp)`

This MATLAB work shows the grayscale picture I in a figure.

`title(['Updated Mask no. ', num2str(idx)])`.

f) Spinal cord mask detection by f_1, f_2, f_3 and f_4 fitness functions:

Trace by f_1

```
u = (updated_mask(:,2) | 0*updated_mask(:,3))
```

the cluster mask for iso intense, (mask no. 2)

$\alpha=2$

Radius of the window for calculating score.

```
temp=[zeros(1,sum([1:w]<y_ant))u(1,y_ant:y_post)zeros(1,
sum[1:w]>y_post)]
```

$S = \text{sum}(A)$ returns the amount of the components of A along the main exhibit measurement whose size doesn't approach 1.

```
q_yz=sum(im2col(temp,[1, 2*alpha+1],'sliding'))
```

$B = \text{im2col}(A,[m \ n],\text{'sliding'})$ or

$B = \text{im2col}(A,[m \ n])$ improves sliding picture neighborhoods of size m -by- n into sections with no zero-cushioning, and returns the connected segments in grid B .

```
temp=[zeros(1,sum([1:w]<y_ant))u(1,y_ant:y_post)zeros(1,
sum[1:w]>y_post)];
```

```
temp=[zeros(1, alpha) temp zeros(1, alpha)];
```

```
for idx_z=z_sup+1:z_inf
```

```
[~,b_z(z_inf)]=max(q_yz)
```

Now scaled up the dimension range from 0-255.

```
Is=255*I
```

$\beta=3$

```
f_yz=sum(255^2-diff(im2col(temp,[1,
2*beta+1],'sliding')).^2)
```

$Y = \text{diff}(X)$ calculates differences between adjacent elements of X along the first array dimension whose size does not equal to 1.

```
idx_shift=[0 -1 1];
```

```
[max_pre_q, idx_p]=max(temp(1+idx_y+idx_shift));
```

```
p_yz(idx_z,idx_y)=idx_shift(idx_p);
```

```
q_yz(idx_y)=max_pre_q+f_yz(idx_y);
```

```
Is=255*I
```

```
y_ant=max(0, b_z-20);
```

```
y_post=min(w, b_z+20);
```

Trace by f_2 ,

```
y_ant=max(0, b2_z-15);
```

```
y_post=max(0, b2_z-1);
```

PLL detection from f_3 fitness function,

```
y_ant=min(w, b2_z+1);
```

```
y_post=min(w, b2_z+15);
```

LF detection from f_4 fitness function,

```
spinal_cord_mask= repmat(1:w,[h,1])
```

$B = \text{repmat}(A,n)$ returns an array containing n copies of A in the row and column dimensions.

g) Elimination of boundary and tumor detection:

```
tumor_mask=bwareaopen(tumor_mask.*imdilate(spinal_cord_mask,
al_trace_f2,strel('disk',3, 6)), 15)
```

$BW2 = \text{bwareaopen}(BW,P)$ orders eliminates every single associated part (protests) that have less than P pixels from the parallel picture BW and delivering another paired picture, $BW2$. This activity is known as a space opening.

```
imshow(imoverlay(I_org,tumor_mask,[1 .3 .3]))
```

Imoverlay burns binary mask into 2-D image. $B = \text{imoverlay}(A,BW)$ fills the grayscale or RGB input picture, A , with a strong shading.

```
disp([num2str(100*sum(tumor_mask(:))/(h*w)), '% pixels are
detected as probable tumor location'])
```

h) Calculating the Tumor Area:

By utilizing 'max' order, we ascertain the biggest components along various dimensional exhibit of the distinguished tumor. Then, at that point we utilize a circle for computing the space of tumor cross-segment.

```
For i = 1:kk
```

```
tumor_area = tumor_area + stats (i). Area;
```

```
end
```

'For' order achieve square of code which determined the occasions and 'end' order end the square of code or demonstrate last cluster file.

3. Result and Discussion

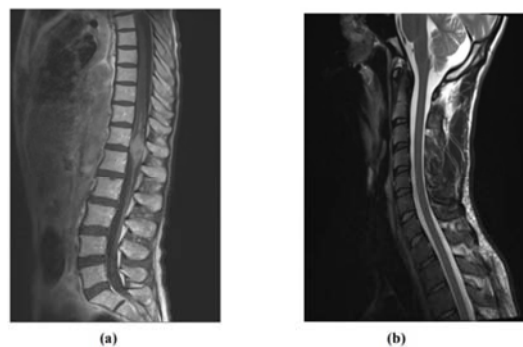


Figure 2. Input of a sample MRI image (a) is tumor affected patient and (b) is normal patient.

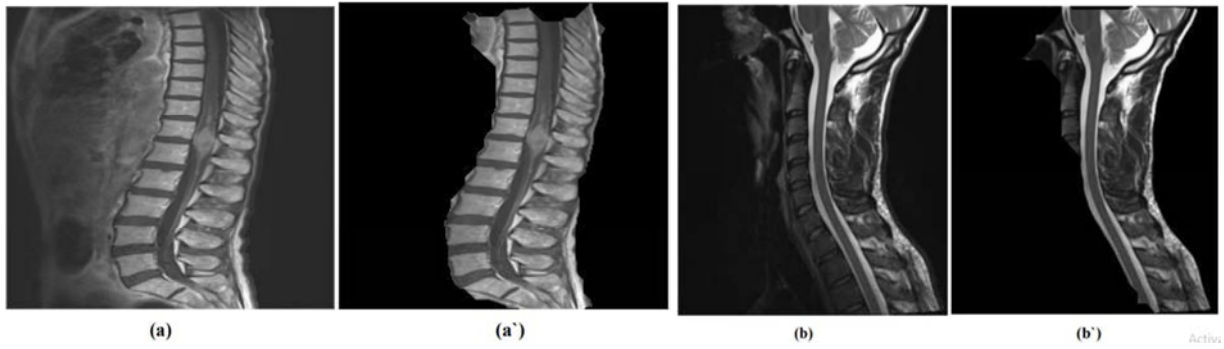


Figure 3. Resized image with region of interest (a) tumor affected patient and (b) normal patient.

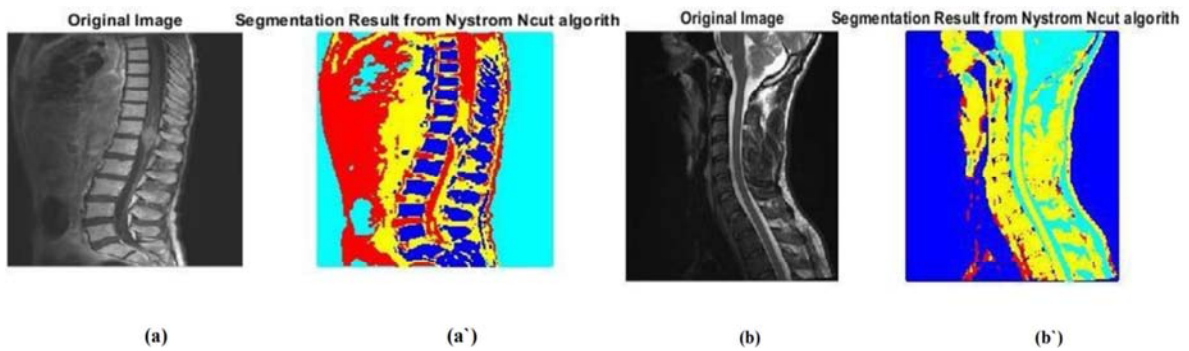


Figure 4. Segmentation result of the input image (a) tumor affected patient and (b) normal patient.

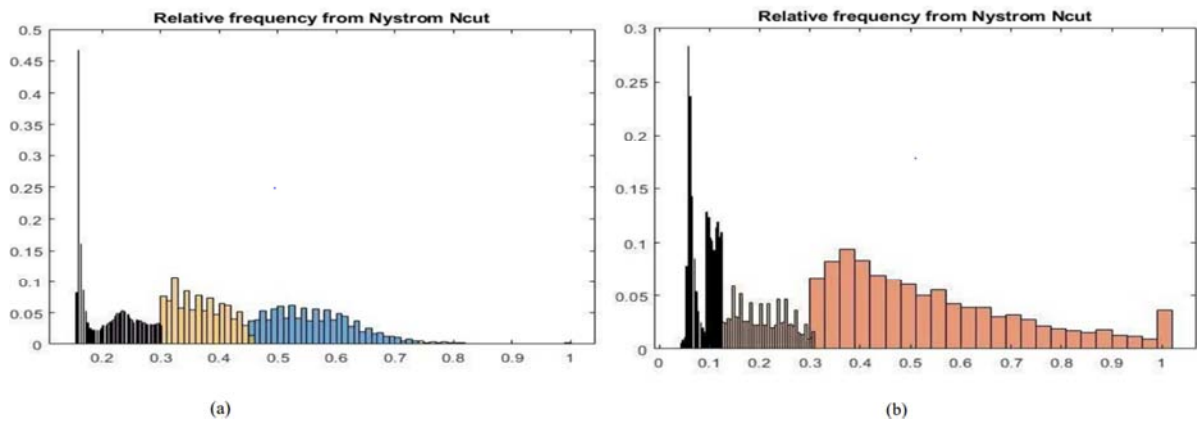


Figure 5. Segmentation representation of the image (a) tumor affected patient and (b) normal patient.

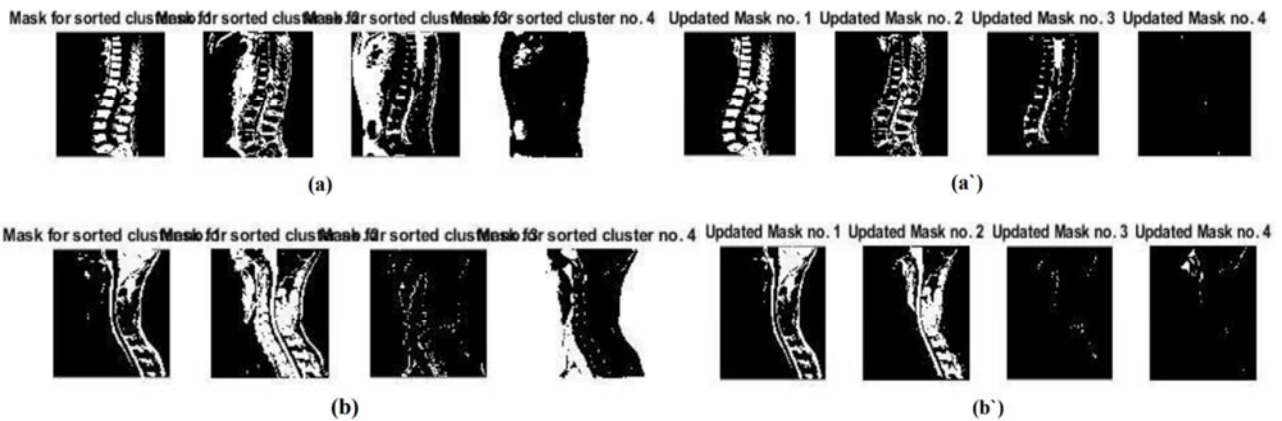


Figure 6. Changing picture for identifying tumor (a) and (b) done by power level (.55,.8), changing picture for distinguishing perimeter(a') and (b') done by force level (.11,.5).

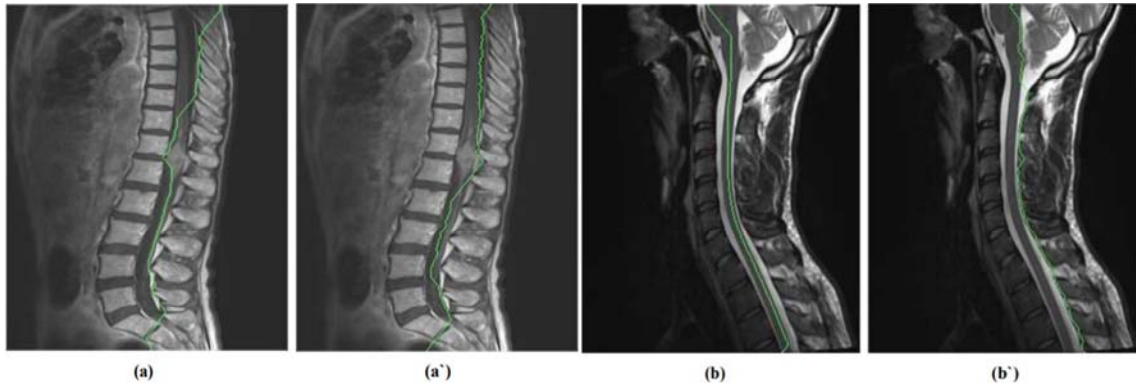


Figure 7. Boundary outline and trace fitness detection from SC to LF.

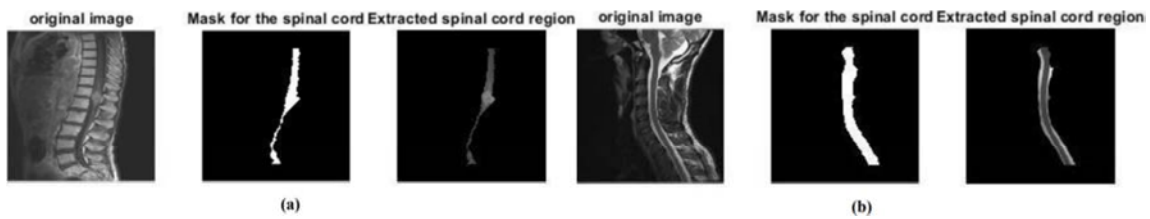


Figure 8. Extracted spinal cord region with mask for the spinal cord of input image (a) tumor affected patient and (b) normal patient.

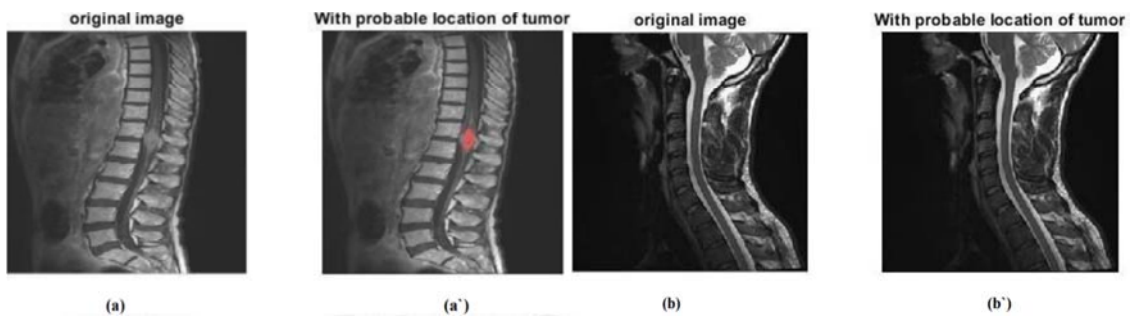


Figure 9. Output image for (a) tumor affected patient and (b) normal patient.

4. Conclusion

In this paper spine tumor recognition method utilizing MRI has been examined. To distinguish tumor MATLAB program framework was planned and to recognize tumor different execution boundaries were utilized like picture histogram and picture profile. On top of that spine tumor influenced region was likewise determined [6-7]. In future work we might want to further develop the sifting technique that has been presently utilized. Powerful sifting strategy will guarantee to distinguish tumor precisely. In future augmentation we will attempt to consolidate technique to distinguish various sorts of tumors (for example Amiable tumor, Milligan tumor, Glioma) [14-16]. We trust that the new augmentations will ready to advise us in what area of the spine is influenced by tumor.

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